

EXHIBIT 17



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United States Patent [19]

Dean et al.

[11] **Patent Number:** 5,561,220[45] **Date of Patent:** * Oct. 1, 1996[54] **TECHNETIUM-99M LABELED PEPTIDES FOR IMAGING INFLAMMATION**[75] **Inventors:** Richard T. Dean; Brian R. Moyer, both of Bedford, N.H.[73] **Assignee:** Diatech, Inc., Londonderry, N.H.[*] **Notice:** The portion of the term of this patent subsequent to Feb. 19, 2013, has been disclaimed.[21] **Appl. No.:** 73,577[22] **Filed:** Jun. 7, 1993**Related U.S. Application Data**

[63] Continuation-in-part of Ser. No. 19,864, Feb. 19, 1993, Pat. No. 5,412,477, which is a continuation-in-part of Ser. No. 653,012, Feb. 8, 1991, abandoned.

[51] **Int. Cl.⁶** A61K 38/00; A61K 51/00; C07F 13/00[52] **U.S. Cl.** 424/1.69; 530/300; 530/326; 436/808; 534/14; 534/10[58] **Field of Search** 530/326, 382, 530/300; 424/1.37, 1.69, 1.73, 1.11; 436/808; 534/14, 10[56] **References Cited****U.S. PATENT DOCUMENTS**

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This invention relates to compositions that are radiolabeled scintigraphic imaging agents, comprising a polybasic compound covalently linked to a radiolabel binding moiety and the composition further comprising a polysulfated glycan. The invention also provides methods for producing and using such compositions. Specifically, the invention relates to compositions comprised of technetium-99m (Tc-99m) labeled scintigraphic imaging agents comprising a polybasic compound having at least 5 chemical functionalities that are basic at physiological pH and a radiolabel-binding moiety, the composition further comprising a polysulfated glycan, the composition being capable of specifically binding to inflammatory sites in vivo. Methods and kits for making such compositions, and methods for using such compositions to image sites of infection and inflammation in a mammalian body, are also provided.

TECHNETIUM-99M LABELED PEPTIDES FOR IMAGING INFLAMMATION

This is a continuation-in-part of U.S. patent application Ser. No. 08/019,864, filed Feb. 19, 1993, now U.S. Pat. No. 5,412,477, which is a continuation-in-part of U.S. patent application Ser. No. 07/653,012, filed on Feb. 8, 1991, now abandoned.

BACKGROUND OF THE INVENTION

1. Field of the Invention

This invention relates to compositions that are radiolabeled scintigraphic imaging agents, methods of using these compositions and methods for producing such radiolabeled compositions. Specifically, the invention relates to technetium-99m labeled scintigraphic imaging agents that are compositions of a polysulfated glycan or mixture thereof and a compound comprising a polybasic moiety covalently linked to a radiolabel binding moiety radiolabeled with technetium-99m (Tc-99m). Methods and kits for making such compositions, and methods for using such compositions to image sites of infection and inflammation in a mammalian body are also provided.

2. Description of the Prior Art

There is a clinical need to be able to determine the location and/or extent of sites of focal or localized infection and inflammation. In a substantial number of cases conventional methods of diagnosis (such as physical examination, x-ray, CT and ultrasonography) fail to identify such sites (e.g., an abscess). Although biopsy may be resorted to, it is preferable to avoid such invasive procedures, at least until they are diagnostically appropriate to identify the pathogen responsible for an abscess at a known location. Identifying the site of such "occult" infection is important because rapid localization and identification of the problem is critical to effective therapeutic intervention.

In the field of nuclear medicine, certain pathological conditions can be localized or the extent of such conditions determined by imaging the internal distribution of administered radioactively-labeled tracer compounds (i.e. radiotracers or radiopharmaceuticals) that accumulate specifically at the pathological site. A variety of radionuclides are known to be useful for radioimaging, including ^{67}Ga , $^{99\text{m}}\text{Tc}$ (Tc-99m), ^{111}In , ^{123}I , ^{125}I , ^{169}Yb and ^{186}Re .

However, an abscess may be caused by any one of many possible pathogens, so that a radiotracer specific for a particular pathogen would have limited scope. On the other hand, infection is almost invariably accompanied by inflammation, which is a general response of the body to tissue injury. Therefore, a radiotracer specific for sites of inflammation would be expected to be useful in localizing sites of infection caused by any pathogen, as well as being useful for localizing other inflammatory sites.

One of the main phenomena associated with inflammation is the localization of leukocytes (white blood cells), usually monocytes and neutrophils, at the site of inflammation. A radiotracer specific for leukocytes would be useful in detecting leukocytes at the site of a localized infection. Currently approved nuclear medicine procedures for imaging sites of infection use either indium-111 labeled leukocytes (^{111}In -WBC) (see, e.g. Peters, 1992, J. Nucl. Med. 33: 65-67) or gallium-67 (^{67}Ga) citrate (see, e.g. Ebright et al., 1982, Arch. Int. Med. 142: 246-254). A major disadvantage of using ^{111}In -labeled WBCs is that the preparation of the radiotracer requires a number of technical steps: sterile removal of

autologous blood, sterile isolation of the leukocytes from the blood, sterile labeling of the leukocytes using conditions that do not damage the cells (since damaged WBC are taken up by the reticuloendothelial system when re-injected) and sterile return (re-injection) of the (now labeled) leukocytes to the patient. Furthermore, a delay of 12 to 48 hours between injection and imaging may be required to obtain optimum imaging. While Tc-99m labeled leukocytes have been used to shorten this delay period (see, e.g. Vorne et al., 1989, J. Nucl. Med. 30: 1332-1336), ex-corporeal labeling is still required. A preferred radiotracer would be one that either would label leukocytes in whole blood or would not require removal and manipulation of autologous blood components ex corpora.

Alternatively, ^{67}Ga -citrate can be administered by intravenous injection. However, this compound is not specific for sites of infection or inflammation. Moreover, a delay of up to 72 hours is often required between injection of the radiotracer and imaging. In addition, the γ -(gamma) emissions energies of ^{67}Ga are not well suited to conventional gamma cameras.

Radiolabeled monoclonal and polyclonal antibodies raised against human leukocytes (including monocytes, neutrophils, granulocytes and other cell types) have been developed. Tc-99m labeled antigranulocyte monoclonal antibodies (see, e.g. Lind et al., 1990, J. Nucl. Med. 31: 417-473) and ^{111}In -labeled non-specific human immunoglobulin (see, e.g. LaMuraglia et al., 1989, J. Vasc. Surg. 10: 20-28) have been tested for the detection of inflammation secondary to infection. ^{111}In -labeled IgG shares the disadvantages of ^{111}In -labeled WBC, in that 24-48 hours are required between injection and optimal imaging. In addition, radiolabeled antibodies are difficult to produce and face protracted approval procedures, as they are routinely classified as biologics by regulatory agencies.

Small, readily synthesized molecules are preferred as routinely-used radiopharmaceuticals. There is clearly a need for small synthetic molecules that can be used either to label leukocytes in whole blood (i.e., without the need to isolate the leukocytes from the other components of whole blood) or that can be directly injected into a patient and will image sites of infection and inflammation by localizing at sites where leukocytes have accumulated.

One kind of small, readily synthesized molecule useful in such applications are peptides. The sensitivity of imaging methods using radioactively-labeled peptides is much higher than other techniques known in the art, since the specific binding of the radioactive peptide concentrates the radioactive signal over the area of interest, for example, an inflammatory site. In addition, methods for achieving high-yield chemical synthesis of small peptides is well known in the art.

Radiolabeled peptides, and in particular formyl-methionyl-leucyl-phenylalanyl (fMLF)-containing peptides, have been reported in the prior art.

Zoghbi et al., 1981, J. Nucl. Med. 22: 32 (Abst) disclose formyl peptide chemotactic factors (fMLF) derived from bacteria coupled to ^{111}In -labeled transferrin.

Jiang et al., 1982, Nuklearmedizin 21: 110-113 disclose a chemotactic formylated peptide (fMLF) radiolabeled with ^{125}I .

Fischman et al., 1991, J. Nucl. Med. 32: 482-491 relates to chemotactic formyl peptide (fMLF)— ^{111}In -labeled DTPA conjugates.

EPC 90108734.6 relates to chemotactic formyl peptide (fMLF)— ^{111}In -labeled DTPA conjugates.

U.S. Pat. No. 4,986,979 relates to the use of radiolabeled chemotactic formyl peptides (fMLF) to radiolabel leukocytes ex-corporally via a photoaffinity label.

PCT W090/10463 relates to the use of radiolabeled chemotactic formyl peptides (fMLF) to radiolabel leukocytes ex-corporally via a photoaffinity label.

The use of labeled fMLF peptides known in the aforementioned art suffers from the serious drawback that this peptide causes adverse physiological responses such as superoxide release from neutrophils (Niedel and Cuatrecasas, 1980, *Formyl Peptide Chemotactic Receptors of Leukocytes and Macrophages*, in *Curr. Top. Cell. Reg.* 17: 137-170), and at sufficient doses these compounds can cause leukocytopenia (Jiang et al., 1982, *Nuklearmed.* 21: 110-113).

Another source of inflammatory site-specific peptides is platelet factor 4 is a naturally-occurring chemotactic peptide, consisting of 70 amino acids having a molecular weight of 7800 daltons and known in the prior art to bind to neutrophils and monocytes, cell types known to be associated with sites of inflammation and infection in vivo. Of interest with regard to the present invention, the carboxyl terminus of PF4 is known to bind to polysulfated glycans such as heparin (Loscalzo et al., 1985, *Arch. Biochem. Biophys.* 240: 446-455). In addition, an advantage of PF4 over the fMLF compounds known in the art is that it does not cause superoxide release from neutrophils even at concentrations of 20 μ M (Bebawy et al., 1986, *J. Leukocyte Biol.* 39: 423-434).

Thorbecke & Zucker, 1989, European Patent Application No. 88111962.2 disclose compositions and methods for modulating immune responses comprising administering an immunomodulating amount of platelet factor 4 or peptides derived therefrom.

Deuel et al., 1977, *Proc. Natl. Acad. Sci. USA* 74: 2256-2258 disclose the amino acid sequence of human platelet factor 4.

Deuel et al., 1981, *Proc. Natl. Acad. Sci. USA* 78: 4584-4587 disclose that platelet factor 4 is chemotactic for neutrophils and monocytes in vitro.

Osterman et al., 1982, *Biochem. Biophys. Res. Comm.* 107: 130-135 disclose that the carboxyl-terminal tridecapeptide of platelet factor 4 has chemotactic properties.

Holt & Niewiarowski, 1985, *Sem. Hematol.* 22: 151-163 provide a review of the biochemistry of platelet α -granule proteins, including platelet factor 4.

Goldman et al., 1985, *Immunol.* 54: 163-171 reveal that fMLF receptor-mediated uptake is inhibited in human neutrophils by platelet factor 4 and a carboxyl-terminal dodecapeptide thereof.

Loscalzo et al., *ibid.*, describe the biochemical interaction between platelet factor 4 and glycosaminoglycans such as heparin.

Bebawy et al., *ibid.*, describe the platelet factor 4-mediated chemotactic response of neutrophils in vitro.

Maione et al., 1989, *Science* 247: 77-79 disclose that angiogenesis is inhibited by recombinant human platelet factor 4 and peptide fragments thereof.

The use of chelating agents for radiolabeling polypeptides, and methods for labeling peptides and polypeptides with Tc-99m are known in the prior art and are disclosed in U.S. patent application Ser. No. 07/653,012, filed Feb. 8, 1991 now abandoned; Ser. No. 07/807,062, filed Nov. 27, 1991 now U.S. Pat. No. 5,443,815; co-pending U.S. patent application Ser. No. 07/871,282, filed Apr. 30, 1992; Ser.

No. 07/886,752, filed May 21, 1992 now abandoned; Ser. No. 07/893,981, filed Jun. 5, 1992 now U.S. Pat. No. 5,508,020; Ser. No. 07/955,466, filed Oct. 2, 1992 now abandoned; co-pending U.S. patent application Ser. No. 08/019,864, filed Feb. 19, 1993; and Ser. No. 08/044,825, filed Apr. 8, 1993 now abandoned, and PCT International Applications PCT/US92/00757, PCT/US92/10716, PCT/US93/02320 and PCT/US93/04794, which are hereby incorporated by reference.

SUMMARY OF THE INVENTION

The present invention provides scintigraphic imaging agents that are compositions comprising radioactively-labeled reagents and polysulfated glycans. The compositions of the invention specifically bind to sites of inflammation in vivo. The reagents comprising the compositions of the invention are themselves comprised of polybasic compounds that are capable of specifically localizing at sites of infection or inflammation or components thereof, wherein said compounds are covalently linked to radioisotope, preferably technetium-99m, binding moieties.

It has unexpectedly been found that the combination of a Tc-99m radiolabeled polybasic compound and a polysulfated glycan as provided by the present invention advantageously enables the acquisition of scintigraphic images of focal sites of infection and inflammation in vivo. Administration of this combination results in a greater degree of localization of the Tc-99m radioactive signal at the site of infection when compared to administration of the Tc-99m labeled polybasic compound alone. As a result, such scintigraphic images produced by this combination are superior to the images obtained using Tc-99m labeled scintigraphic imaging agents comprising the radiolabeled polybasic compound alone (see Example 3 and Table II hereinbelow). Higher ratios of the detected radioactivity at infection site versus blood and infection site versus normal tissue are also found using the compositions of the invention compared with the radiolabeled compounds alone.

Accordingly, the invention provides radiolabeled compositions that bind to sites of inflammation in vivo, methods for preparing such compositions, and methods for using such radiolabeled compositions for imaging sites of infection and inflammation within a mammalian body.

In a first aspect of the present invention, scintigraphic imaging agents for imaging sites of inflammation within a mammalian body are provided, comprising compositions that comprise a technetium-99m labeled reagent having a molecular weight of about 500 daltons to about 15,000 daltons and having at least 5 residues that are basic at physiological pH, covalently linked to a technetium-99m binding moiety, the composition further comprising a polysulfated glycan having a molecular weight of about 1000 daltons to about 60,000 daltons, wherein the reagent is radioactively labeled with technetium-99m, and wherein the composition is capable of binding to sites of inflammation in vivo. In preferred embodiments, the reagent is a peptide of 5 to 100 amino acids that is platelet factor 4 or a fragment or analog thereof. In other preferred embodiments, the polysulfated glycan is heparin, heparan sulfate, dextran sulfate, chondroitin sulfate, dermatan sulfate or derivatives thereof.

In a second aspect of the invention, Tc-99m labeled reagents are provided as components of the scintigraphic imaging agents of the invention, wherein the reagents are comprised of polybasic compound, preferably a platelet

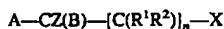
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factor 4-derived peptide of fragment thereof, covalently linked to a radiolabel-binding moiety of formula



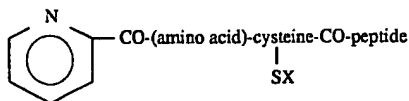
wherein Cp is a protected cysteine residue and (aa) stands for an amino acid, and wherein the radiolabel-binding moiety is covalently linked to the polybasic compounds. In a preferred embodiment, the amino acid is glycine. In another preferred embodiment, the radiolabel-binding moiety is linked to the polybasic compound via from about one to about 20 amino acids.

In a third aspect, a component of the scintigraphic imaging agents provided by the invention are reagents comprising a polybasic compound, preferably a platelet factor 4-derived peptide of fragment thereof, covalently linked to a radiolabel-binding moiety having the following structure:

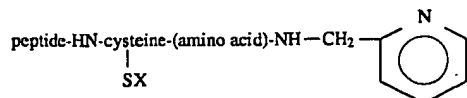


wherein A is H, HOOC, H₂NOC, (peptide)-NHOC, (peptide)-OOC or R⁴; B is H, SH or —NHR³, —N(R³)-(peptide) or R⁴; X is SH or —NHR³, —N(R³)-(peptide) or R⁴; R¹, R², R³ and R⁴ are independently H or straight or branched chain or cyclic lower alkyl; n is 0, 1 or 2; and: (1) where B is —NHR³ or —N(R³)-(peptide), X is SH and n is 1 or 2; (2) where X is —NHR³ or —N(R³)-(peptide), B is SH and n is 1 or 2; (3) where B is H or R⁴, A is HOOC, H₂NOC, (peptide)-NHOC, (peptide)-OOC, X is SH and n is 0 or 1; (4) where A is H or R⁴, then where B is SH, X is —NHR³ or —N(R³)-(peptide) and where X is SH, B is —NHR³ or —N(R³)-(peptide); (5) where X is H or R⁴, A is HOOC, H₂NOC, (peptide)-NHOC, (peptide)-OOC and B is SH; (6) where Z is methyl, X is methyl, A is HOOC, H₂NOC, (peptide)-NHOC, (peptide)-OOC and B is SH and n is 0; and (7) where Z is SH and X is SH, n is not 0; and wherein the thiol moiety is in the reduced form.

In another embodiment are provided components of the scintigraphic imaging agents of the invention comprising a reagent comprised of a polybasic compound, preferably a platelet factor 4-derived peptide of fragment thereof, covalently linked to a radiolabel-binding moiety of formula:



[for purposes of this invention, radiolabel-binding moieties having this structure will be referred to as picolinic acid (Pic)-based moieties];
or

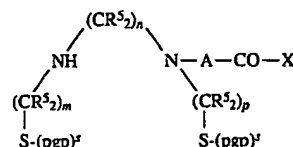


[for purposes of this invention, radiolabel-binding moieties having this structure will be referred to as picolylamine (Pica)-based moieties]; wherein X is H or a protecting group; (amino acid) is any amino acid; the radiolabel-binding moiety is covalently linked to the peptide and the complex of the radiolabel-binding moiety and the radiolabel is electrically neutral. In a preferred embodiment, the amino acid is glycine and X is an acetamidomethyl protecting group. In additional preferred embodiments, the polybasic compound is covalently linked to the radiolabel-binding

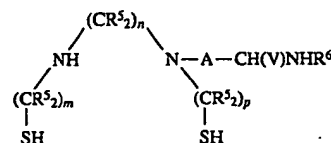
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moiety via an amino acid, most preferably glycine, and the radiolabel is technetium-99m.

In yet another embodiment of the invention, components of the radiolabeled scintigraphic imaging agents of the invention are provided that are reagents comprising a polybasic compound, preferably a platelet factor 4-derived peptide or fragment thereof, and a bisamino bisthiol radiolabel-binding moiety covalently linked to the polybasic compound. The bisamino bisthiol radiolabel-binding moiety in this embodiment of the invention has a formula selected from the group consisting of:



wherein each R⁵ can be independently H, CH₃ or C₂H₅; each (pgp)s can be independently a thiol protecting group or H; m, n and p are independently 2 or 3; A is linear or cyclic lower alkyl, aryl, heterocyclyl, combinations or substituted derivatives thereof; and X is peptide;



wherein each R⁵ is independently H, lower alkyl having 1 to 6 carbon atoms, phenyl, or phenyl substituted with lower alkyl or lower alkoxy; m, n and p are independently 1 or 2; A is linear or cyclic lower alkyl, aryl, heterocyclyl, combinations or substituted derivatives thereof; V is H or CO-peptide; R⁶ is H or peptide; provided that when V is H, R⁶ is peptide and when R⁶ is H, V is peptide. [For purposes of this invention, radiolabel-binding moieties having these structures will be referred to as "BAT" moieties]. In a preferred embodiment, the polybasic compound is covalently linked to the radiolabel-binding moiety via an amino acid, most preferably glycine.

The invention also comprises kits for preparing the compositions of the invention, methods for radiolabeling the reagents of the invention with Tc-99m and methods for using the radiolabeled compositions for imaging sites of infection or inflammation in mammalian body by gamma scintigraphy.

The invention provides compositions that are scintigraphic imaging agents comprising complexes of the radiolabel binding moiety of the reagents of the invention with Tc-99m. Methods for radiolabeling these reagents with Tc-99m are also provided. Radiolabeled complexes provided by the invention are formed by reacting the reagents of the invention with Tc-99m in the presence of a reducing agent. Preferred reducing agents include but are not limited to dithionite ion, stannous ion and ferrous ion. Complexes of the invention are also formed by labeling by ligand exchange of a prereduced Tc-99m complex as provided herein.

The invention also provides kits for preparing scintigraphic imaging agents that are a composition comprising a polysulfated glycan and Tc-99m labeled reagents of the invention. Kits for preparing the scintigraphic imaging agents of the invention, wherein the radiolabel is Tc-99m, are comprised of a first sealed vial containing a predetermined quantity of an unlabeled embodiment of a reagent of the invention and a sufficient amount of reducing agent to label the reagent with technetium-99m, and a second sealed

vial containing a predetermined quantity of the polysulfated glycan of the invention. Compositions of the invention are then made by labeling the contents of the first vial with technetium-99m and then mixing the contents of the first vial with the contents of the second vial to provide the composition. Alternatively, appropriate amounts of the unlabeled reagent and the polysulfated glycan can be contained in a single vial. In preferred embodiments, the polysulfated glycan is heparin, heparan sulfate, dextran sulfate, chondroitin sulfate, dermatan sulfate or derivatives thereof.

This invention provides methods for preparing peptide embodiments of the scintigraphic imaging agents of the invention by chemical synthesis *in vitro*. In a preferred embodiment, peptides are synthesized by solid phase peptide synthesis.

This invention provides methods for using compositions comprising Tc-99m labeled scintigraphic imaging agents for imaging sites of inflammation and infection within a mammalian body by obtaining *in vivo* gamma scintigraphic images. These methods comprise administering an effective diagnostic amount of a Tc-99m labeled composition and detecting the gamma radiation emitted by the Tc-99m label localized at the inflammation site within the mammalian body.

Methods are also provided for specifically radiolabeling whole blood and using mixtures comprising radiolabeled whole blood to image sites of inflammation within a mammalian body. One such embodiment comprises mixing whole blood with an amount, preferably from about 1 microgram to 100 milligrams, of a polysulfated glycan to form a mixture. A radiolabeled whole blood mixture is then formed by adding an amount, from about 1 microgram to 100 milligrams, of a radiolabeled, preferably Tc-99m labeled, composition of matter that is a reagent comprising a polybasic moiety covalently linked to a radiolabel binding moiety, to the first whole blood mixture. This radiolabeled whole blood mixture is then administered to an animal such as a human being having or suspected of having a site of inflammation *in vivo*, and the radioactive signal detected to localize the site of inflammation as described herein. This method provides an advantage over methods for labeling leukocytes known in the prior art, since the instant method eliminates the need for isolation of leukocytes from whole blood and attendant extensive *ex corpora* manipulation of whole blood.

The reagents of the invention may also be comprised of a polyvalent linking moiety. Polyvalent linking moieties of the invention are comprised of at least 2 identical linker functional groups capable of covalently bonding to polybasic compounds or Tc-99m binding moieties. Preferred linker functional groups are primary or secondary amines, hydroxyl groups, carboxylic acid groups or thiol-reactive moieties. In preferred embodiments, the polyvalent linking moieties are comprised of bis-succinimidylmethylether (BSME), 4-(2,2-dimethylacetyl)benzoic acid (DMBA), N-[2-(N',N'-bis(2-succinimido-ethyl)aminoethyl)]-N⁶,N⁹-bis(2-methyl-2-mercaptopropyl)-6,9-diazanonanamide (BAT-BS), tris(succinimidylethyl)amine (TSEA), bis-succinimidohexane (BSH), 4-(O-CH₂CO-Gly-Gly-Cys.amide)acetophenone (ETAC) or a derivative thereof.

Specific preferred embodiments of the present invention will become evident from the following more detailed description of certain preferred embodiments and the claims.

DETAILED DESCRIPTION OF THE INVENTION

The present invention provides scintigraphic imaging agents for imaging target sites within a mammalian body

that specifically bind to sites of inflammation comprising compositions of Tc-99m labeled reagents and polysulfated glycans. The reagents of the compositions of the invention comprise polybasic compounds that are covalently linked to a radiolabel binding moiety wherein the radiolabel binding moiety binds a radioisotope. For the purposes of this invention, the term "polybasic compound" is intended to encompass chemical compounds having at least 5 chemical functionalities that are basic and are cationic at physiological pH (i.e. about pH 7.0 \pm 0.5), for example but not limited to, primary amines, whereby said polybasic compounds are polycationic at physiological pH. Polysulfated glycans of the invention include but are not limited to heparin, heparan sulfate, dextran sulfate, chondroitin sulfate, dermatan sulfate or derivatives thereof.

The compositions of this invention specifically localize to sites of inflammation. These compositions may also bind to leukocytes, preferably monocytes and neutrophils and most preferably to neutrophils. For purposes of this invention, the term "bind to leukocytes" is intended to mean that the compositions of the invention are capable of accumulating at sites of infection or inflammation in mammalian body sufficient to allow detection of the accumulation of radiolabeled complexes prepared from the compositions as disclosed herein at sites of infection or inflammation by gamma scintigraphy.

In peptide embodiments of the scintigraphic imaging agents of the invention, preferred peptides include platelet factor 4 and peptides derived therefrom. For purposes of this invention, the term "peptides derived therefrom" is intended to encompass peptides having an amino acid sequence homologous to all or a portion of the platelet factor 4 amino acid sequence. Also intended to be circumscribed by this term are peptide fragments of platelet factor 4, whether generated by proteolytic degradation of native platelet factor 4 protein or by chemical synthesis of a portion of the platelet factor 4 amino acid sequence. Peptide fragments useful in the practice of this invention include those fragments capable of specifically binding to sites of infection and inflammation in a mammalian body. Examples of such peptides are presented hereinafter in the Examples.

In Cp(aa)Cp-containing scintigraphic imaging agents, the Cp is a protected cysteine where the S-protecting groups are the same or different and may be but not limited to:

- CH₂-aryl (aryl is phenyl or alkyl or alkyloxy substituted phenyl);
- CH-(aryl)₂, (aryl is phenyl or alkyl or alkyloxy substituted phenyl);
- C-(aryl)₃, (aryl is phenyl or alkyl or alkyloxy substituted phenyl);
- CH₂-(4-methoxyphenyl);
- CH—(4-pyridyl)(phenyl)₂;
- C(CH₃)₃
- 9-phenylfluorenyl;
- CH₂NHCOR (R is unsubstituted or substituted alkyl or aryl);
- CH₂NHCOOR (R is unsubstituted or substituted alkyl or aryl);
- CONHR (R is unsubstituted or substituted alkyl or aryl);
- CH₂—S—CH₂-phenyl.

Radiolabel binding moieties comprising cysteine-sulfur protecting groups designated "(pgp)"⁵, such as the bisamino, bithiol moieties of the invention, are also described by the above-mentioned listing of protecting groups.

The preferred protecting group has the formula $\text{—CH}_2\text{—NHCOR}$ wherein R is a lower alkyl having 1 and 8 carbon atoms, phenyl or phenyl-substituted with lower alkyl, hydroxyl, lower alkoxy, carboxy, or lower alkoxycarbonyl.

Labeling with Tc-99m is an advantage of the present invention because the nuclear and radioactive properties of this isotope make it an ideal component of a scintigraphic imaging agent. This isotope has a single photon energy of 140 keV and a radioactive half-life of about 6 hours, and is readily available from a ^{99}Mo - $^{99\text{m}}\text{Tc}$ generator. Other radionuclides known in the prior art have effective half-lives which are much longer (for example, ^{111}In , which has a half-life of 67.4 h) or are toxic (for example, ^{125}I).

Each polybasic peptide-containing embodiment of the invention is comprised of a sequence of amino acids. The term amino acid as used in this invention is intended to include all L- and D-amino acids, naturally occurring and otherwise. Reagents comprising polybasic peptides provided by the invention include but are not limited to the following (the amino acids in the following peptides are L-amino acids except where otherwise indicated):

acetyl-KC_{Acm}GC_{Acm}QAPLYKKI_{KKLLES}
 acetyl-KKC_{Acm}GC_{Acm}QAPLYKKI_{KKLLES}
 acetyl-KKKC_{Acm}GC_{Acm}QAPLYKKI_{KKLLES}
 acetyl-KKKKC_{Acm}GC_{Acm}QAPLYKKI_{KKLLES}
 acetyl-KKKKC_{Acm}GC_{Acm}QAPLYKKI_{KKLLES}
 acetyl-KC_{Acm}GC_{Acm}GGPLYKKI_{KKLLES}
 acetyl-KKC_{Acm}GC_{Acm}GGPLYKKI_{KKLLES}
 acetyl-KKKC_{Acm}GC_{Acm}GGPLYKKI_{KKLLES}
 acetyl-KKKKC_{Acm}GC_{Acm}GGPLYKKI_{KKLLES}
 acetyl-KKKKC_{Acm}GC_{Acm}GGPLYKKI_{KKLLES}

Polybasic peptide embodiments of the present invention may be chemically synthesized *in vitro*. Peptides of the present invention can generally advantageously be prepared on a peptide synthesizer. The peptides of this invention can be synthesized wherein the radiolabel binding moiety is covalently linked to the peptide during chemical *in vitro* synthesis, using techniques well known to those with skill in the art. Such peptides covalently-linked to the radiolabel binding moiety upon synthesis are advantageous because specific sites of covalent linkage can be determined therein.

Radiolabel binding moieties of the invention may be introduced into the target specific polybasic peptide during peptide synthesis. For embodiments [e.g., Pic-Gly-Cys(protecting group)-] comprising picolinic acid (Pic-), the radiolabel-binding moiety can be synthesized as the last (i.e., amino-terminal) residue in the synthesis. In addition, the picolinic acid-containing radiolabel-binding moiety may be covalently linked to the α -amino group of lysine to give, for example, $\alpha\text{N}(\text{Fmoc})\text{-Lys-}\epsilon\text{N}[\text{Pic-Gly-Cys(protecting group)}]$, which may be incorporated at any position in the peptide chain. This sequence is particularly advantageous as it affords an easy mode of incorporation into the target binding peptide.

Similarly, the picolylamine (Pica)-containing radiolabel-binding moiety [-Cys(protecting group)-Gly-Pica] can be prepared during peptide synthesis by including the sequence [Cys(protecting group)-Gly-] at the carboxyl terminus of the peptide chain. Following cleavage of the peptide from the resin the carboxyl terminus of the peptide is activated and coupled to picolylamine. This synthetic route requires that reactive side-chain functionalities remain masked (protected) and do not react during the conjugation of the picolylamine.

This invention provides for the incorporation of these chelators into virtually any platelet factor 4-derived peptide, resulting in Tc-99m radiolabeled peptide components of the scintigraphic imaging agents of the invention.

This invention also provides polybasic, small, synthetic compounds which incorporate bisamine bithiol (BAT) chelators which may be labeled with Tc-99m.

In forming a complex of radioactive technetium-99m with the reagents of this invention, the technetium complex, preferably a salt of Tc-99m pertechnetate, is reacted with the imaging agent in the presence of a reducing agent; in a preferred embodiment, the reducing agent is stannous chloride. Complexes and means for preparing such complexes are conveniently provided in a kit form comprising a first sealed vial containing a predetermined quantity of a reagent of the invention that is to be labeled and a sufficient amount of reducing agent to label the reagent with Tc-99m. Alternatively, the complex may be formed by reacting a reagent of the invention with a pre-formed labile complex of technetium and another compound known as a transfer ligand. This process is known as ligand exchange and is well known to those skilled in the art. The labile complex may be formed using such transfer ligands as tartrate, citrate, gluconate or mannitol, for example. Among the Tc-99m pertechnetate salts useful with the present invention are included the alkali metal salts such as the sodium salt, or ammonium salts or lower alkyl ammonium salts. Using either embodiment, the vial containing the unlabeled reagent and reducing agent can also advantageously contain the polysulfated glycan components of the compositions of the invention. The reaction of the scintigraphic imaging agents of this invention with Tc-99m pertechnetate or preformed Tc-99m labile complex can be carried out in an aqueous medium at room temperature. When an anionic complex is formed in an aqueous medium, the radiolabeled complex is in the form of a salt with a suitable cation such as sodium cation, ammonium cation, mono, di- or tri-lower alkyl amine cation, or any pharmaceutically acceptable cation.

In a preferred embodiment of the invention, a kit for preparing technetium-99m labeled peptides is provided. The peptide embodiments of the reagents of the invention can be chemically synthesized using methods and means well-known to those with skill in the art and described hereinbelow. An appropriate amount of such a reagent is introduced into a vial containing a reducing agent, such as stannous chloride or a solid-phase reducing agent, in an amount sufficient to label the agent with Tc-99m. An appropriate amount of a transfer ligand as described (such as tartrate, citrate, gluconate or mannitol, for example) can also be included. Technetium-99m labeled reagents according to the present invention can be prepared by the addition of an appropriate amount of Tc-99m or Tc-99m complex into the vials and reaction under conditions described in Example 2 hereinbelow. Said kits also comprise a second sealed vial containing an appropriate amount of a polysulfated glycan. Examples of efficacious polysulfated glycans include but are not limited to heparin, heparan sulfate, dextran sulfate, chondroitin sulfate, dermatan sulfate or derivatives thereof. Tc-99m labeled scintigraphic imaging agents of the invention can be prepared by mixing the Tc-99m labeled polybasic component from the first vial with the polysulfated glycan from the second vial.

Radioactively labeled scintigraphic imaging agents provided by the present invention are provided having a suitable amount of radioactivity. In forming the Tc-99m radioactive complexes, it is generally preferred to form radioactive complexes in solutions containing radioactivity at concentrations of from about 0.01 millicurie (mCi) to 100 mCi per ml.

Compositions comprising scintigraphic imaging agents comprised of technetium-99m labeled reagents and polysulfated glycans provided by this invention can be used for visualizing sites of inflammation, including abscesses and sites of "occult" infection. The Tc-99m labeled compositions can also be used for visualizing sites of inflammation caused by tissue ischemia, including such disorders as inflammatory bowel disease and arthritis. In accordance with this invention, the technetium-99m labeled compositions, wherein the reagents are provided either as a complex or as a salt with a pharmaceutically acceptable counterion, are administered in a single unit injectable dose. Any of the common carriers known to those with skill in the art, such as sterile saline solution or plasma, can be utilized after radiolabeling for preparing the injectable solution to diagnostically image various organs, tumors and the like in accordance with this invention. Generally, the unit dose to be administered has a radioactivity of about 0.01 mCi to about 100 mCi, preferably 1 mCi to 20 mCi. The composition to be injected at unit dosage is from about 0.01 ml to about 10 ml. After intravenous administration, imaging of the organ or tumor in vivo can take place in a matter of a few minutes. However, imaging can take place, if desired, in hours or even longer, after injecting into patients. In most instances, a sufficient amount of the administered dose will accumulate in the area to be imaged within about 0.5 of an hour to permit the taking of scintiphotos. Any conventional method of scintigraphic imaging for diagnostic purposes can be utilized in accordance with this invention.

The technetium-99m labeled compositions of the invention may be administered intravenously in any conventional medium for intravenous injection such as an aqueous saline medium, or in blood plasma medium. Such medium may also contain conventional pharmaceutical adjunct materials such as, for example, pharmaceutically acceptable salts to adjust the osmotic pressure, buffers, preservatives and the like. Among the preferred media are normal saline and plasma.

Alternatively, the invention provides methods for specifically radiolabeling whole blood and using such radiolabeled whole blood to image sites of inflammation within a mammalian body. In this embodiment of the invention, whole blood is mixed with an amount, from about 1 microgram to 100 milligrams, of a polysulfated glycan to form a mixture. Then an amount, from about 1 microgram to 100 milligrams, of a radiolabeled, preferably Tc-99m labeled, composition of matter that is a reagent comprising a polybasic moiety covalently linked to a radiolabel binding moiety, is added to form a radiolabeled mixture. This radiolabeled whole blood mixture is then administered to an animal such as a human being having or suspected of having a site of inflammation in vivo, and the radioactive signal detected to localize the site of inflammation as described herein. The requirement for antigenically-compatible, preferably but not necessarily autologous, heparinized whole blood to be used in this embodiment of the experiment will be understood by those skilled in the art.

The methods for making and labeling these compositions are more fully illustrated in the following Examples. These Examples illustrate certain aspects of the above-described method and advantageous results. These Examples are shown by way of illustration and not by way of limitation.

EXAMPLE 1

Solid Phase Peptide Synthesis

Solid phase peptide synthesis (SPPS) was carried out on a 0.25 millimole (mmole) scale using an Applied Biosystems Model 431A Peptide Synthesizer and using 9-fluorenylmethoxycarbonyl (Fmoc) amino-terminus protection, coupling with dicyclohexylcarbodiimide/hydroxybenzotriazole or 2-(1H-benzo-triazol-1-yl)-1,13,3-tetramethyluronium hexafluorophosphate/hydroxybenzotriazole (HBTU/HOBT), and using p-hydroxymethylphenoxymethylpolystyrene (HMP) resin for carboxyl-terminus acids or Rink amide resin for carboxyl-terminus amides.

Where appropriate N- α -acetyl groups were introduced by treating the resin-bound peptide with acetic anhydride in N-methylpyrrolidinone (NMP).

Resin-bound products were routinely cleaved using a solution comprised of trifluoroacetic acid, water, thioanisole, ethanedithiol, and triethylsilane, prepared in ratios of 100:5:5:2.5:2 for 1.5–3 h at room temperature. Crude peptides were purified by preparative high pressure liquid chromatography (HPLC) using a Waters Delta Pak C18 column and gradient elution using 0.1% trifluoroacetic acid (TFA) in water modified with acetonitrile. Acetonitrile was evaporated from the eluted fractions which were then lyophilized. The identity of each product was confirmed by fast atom bombardment mass spectroscopy (FABMS) or by electrospray mass spectroscopy (ESMS).

EXAMPLE 2

A General Method for Radiolabeling with Tc-99m

Peptide (0.1 mg) prepared as in Example 1 was dissolved in 0.1 mL of phosphate buffered saline, 0.05M potassium phosphate buffer (pH 7.4) or water. Tc-99m gluceptate was prepared by reconstituting a Glucoscan vial (E.I. DuPont de Nemours, Inc.) with 1.0 mL of Tc-99m sodium pertechnetate containing up to 200 mCi and allowed to stand for 15 minutes at room temperature. 25 μ L of Tc-99m gluceptate was then added to the peptide reagent and the reaction allowed to proceed at 100° C. or at room temperature for 30 min and then filtered through a 0.2 μ m filter.

The purity of the Tc-99m labeled peptide reagent was determined by HPLC under the conditions described in the footnotes of the following Table. Radioactive components were detected by an in-line radiometric detector linked to an integrating recorder. Tc-99m gluceptate and Tc-99m sodium pertechnetate elute between 1 and 4 minutes under these conditions, whereas the Tc-99m labeled peptide eluted after a much greater amount of time.

The following Table illustrates successful Tc-99m labeling of peptides prepared according to Example 1 using the method described herein.

TABLE I

	FABMS MH ⁺	Radiochemical Yield	HPLC R _t (min)
AcKKKKKC _{Ac} GC _{Ac} GGPLYKKIKKLLS	2276	98%	11.3

TABLE I-continued

Ac = acetyl; Ac_m = acetamidomethyl; single-letter abbreviations for amino acids can be found in G. Zubay, Biochemistry (2d. ed.), 1988 (MacMillan Publishing: New York) p. 33.
General HPLC method:

solvent A = 0.1% CF₃COOH/H₂O
solvent B₉₀ = 0.1% CF₃COOH/90% CH₃CN/H₂O
solvent flow rate = 1.2 mL/min
Vydak column = Vydak 218TP54 RP-18, 5μ × 220 mm + 4.6 mm analytical column with guard column; or
Waters column = Waters Delta-Pak C18 5μ × 39 mm × 150 mm column
Method: Gradient elution 100% A to 100% B₉₀ in 10 min

EXAMPLE 3

Scintigraphic Imaging and Biodistribution of Tc-99m Labeled Peptides

The efficacy of scintigraphic imaging of inflammatory sites in vivo using the composition of the invention was demonstrated as follows. New Zealand white rabbits were inoculated intramuscularly in the left calf with a potent

and that all modifications or alternatives equivalent thereto are within the spirit and scope of the invention as set forth in the appended claims.

TABLE II

Composition	% ID/g: infected muscle		% ID/g: normal muscle		% ID/g: blood		infected muscle/blood		infected muscle/ normal muscle	
	4 h	14 h	4 h	14 h	4 h	14 h	4 h	14 h	4 h	14 h
P322	0.013	0.007	0.003	0.001	0.018	0.006	0.70	1.2	4.9	7.0
P322 + heparin	0.019	0.018	0.004	0.001	0.015	0.010	1.2	1.9	5.0	18.0

strain of *Escherichia coli*. After 24 h, the animals were sedated by intramuscular injection with ketamine and xylazine. The animals were then injected intravenously with Tc-99m labeled peptide (≤ 150 μg peptide/2–10 mCi Tc-99m) alone or in a solution that contained 30 U.S.P. Units/mL heparin. The animals were positioned supine in the field of view of a gamma camera (LEAP collimator, photopeaked for Tc-99m) and imaged over the first hour post-injection, and then at approximately 1 h intervals over the following 3 h or 13 h. Animals were allowed to recover between the times of image acquisition and re-anesthetized as needed.

Upon completion of the final imaging, each animal was sacrificed by phenobarbital overdose induced by i.v. injection, and dissected to obtain samples of blood and of infected and control muscle. These tissue samples were weighed and counted using a gamma counter. A standard amount of the injected dose was also counted in this manner. The percent injected dose (per gram of tissue) remaining in the tissue was calculated from the results of gamma counting. Ratios of percent injected dose per gram of infected versus non-infected muscle tissue, and ratios of percent of injected dose per gram of infected tissue versus blood, were calculated; these results are shown in the following Table.

Rabbits were injected with a Tc-99m labeled imaging agent of the invention, having the formula acetyl-KKKKKC_{Ac_m}GC_{Ac_m}GGPLYKKIHKLLLES. The combination of Tc-99m labeled peptide and heparin resulted in a greater percentage of the injected dose detected in the infected muscle, and higher ratios of infected muscle/blood and infected muscle to normal muscle, than were obtained using the labeled peptide alone (see Table).

It should be understood that the foregoing disclosure emphasizes certain specific embodiments of the invention

What is claimed is:

1. A composition that is a scintigraphic imaging agent for imaging sites of inflammation within a mammalian body, the composition comprising a reagent comprised of a polybasic compound having a molecular weight of about 500 daltons to about 15,000 daltons and having at least 5 chemical functionalities that are basic at physiological pH, covalently linked to a technetium-99m binding moiety, the composition further comprising a polysulfated glycan having a molecular weight of about 1,000 daltons to about 60,000 daltons, wherein the reagent is radioactively labeled with technetium-99m, and wherein the composition is capable of binding to sites of inflammation in vivo.

2. The composition of claim 1 wherein the polybasic compound of the reagent comprising the composition is a peptide of 5 to 100 amino acids that is platelet factor 4 or a fragment thereof.

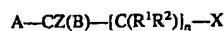
3. The composition of claim 1 wherein the polysulfated glycan is heparin, heparan sulfate, dextran sulfate, chondroitin sulfate, dermatan sulfate or derivatives thereof.

4. The composition of claim 1 wherein the technetium-99m binding moiety is selected from the group consisting of:



I.

wherein Cp is a protected cysteine and (aa) is an amino acid;



II.

wherein

A is H, HOOC, H₂NOC, (peptide)-NHOC, (peptide)-OOC or R⁴;

B is H, SH, —NHR³, —N(R³)-(peptide), or R⁴;

X is H, SH, —NHR³, —N(R³)-(peptide) or R⁴;

Z is H or R⁴;

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R¹, R², R³ and R⁴ are independently H or lower straight or branched chain or cyclic alkyl;

n is 0, 1 or 2; and

where B is —NHR^3 or $\text{—N(R}^3\text{)-(peptide)}$, X is SH, and n is 1 or 2;

where X is —NHR^3 or $\text{—N(R}^3\text{)—(peptide)}$, B is SH, and n is 1 or 2:

where B is H or R⁴, A is HOOC, H₂NOC, (peptide)-NHOC, (peptide)-OOC, X is SH, and n is 0 or 1;

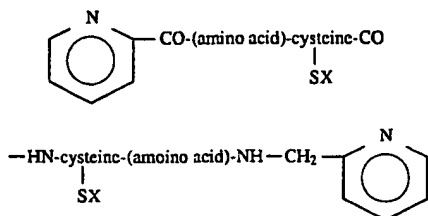
where A is H or R⁴, then where B is SH, X is —NHR³ or —N(R³)-(peptide) and where X is SH, B is —NHR³ or —N(R³)-(peptide);

where X is H or R⁴, A is HOOC, H₂NOC, (peptide)-NHOC, (peptide)-OOC and B is SH;

where Z is methyl, X is methyl, A is HOOC, H₂NOC, (peptide)-NHOC, (peptide)-OOC, B is SH and n is 0;

where B is SH and X is SH, n is not 0;

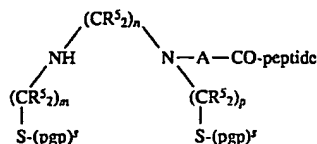
and wherein the thiol moiety is in the reduced form; and



wherein

X=H or a protecting group;

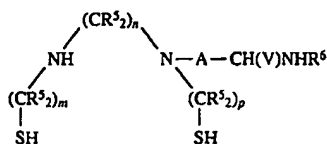
(amino acid)=any amino acid;



wherein each R⁵ is independently H, CH₃ or C₂H₅;

each (pgp)^r is independently a thiol protecting group or H;
m, n and p are independently 2 or 3;

A=linear or cyclic lower alkyl, aryl, heterocyclyl, combinations or substituted derivatives thereof:



wherein

each R⁵ is independently H, lower alkyl having 1 to 6 carbon atoms, phenyl, or phenyl substituted with lower alkyl or lower alkoxy;

m, n and p are independently 1 or 2;

A=linear or cyclic lower alkyl, aryl, heterocyclyl, combinations or substituted derivatives thereof:

V=H or —CO-peptide;

$R^6=H$ or peptide;

and wherein when $V=H$, $R^6=\text{peptide}$ and when $R^6=H$, $V=\text{—CO-peptide}$; wherein the radiolabel-binding moiety forms a complex with a radioisotope and the complex is electrically neutral.

5. The composition of claim 1 wherein the polybasic compound and the radiolabel binding moiety are covalently linked through from about one to about twenty amino acids.

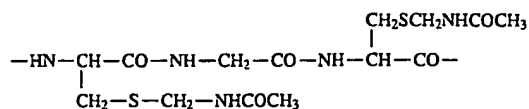
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6. The composition of claim 4 wherein the protected cysteine of the radiolabel-binding moiety comprising the reagent of the composition having formula I has a protecting group of the formula



wherein R is a lower alkyl having 1 to 6 carbon atoms, 2-,3-,4-pyridyl, phenyl, or phenyl substituted with lower alkyl, hydroxy, lower alkoxy, carboxy, or lower alkoxy-carbonyl.

7. The composition of claim 4 wherein the radiolabel-binding moiety of formula Cp(aa)Cp that comprises the reagent of the composition has the formula:



8. The composition of claim 2 wherein the polybasic compound comprising the reagent of the composition is a peptide having an amino acid sequence comprising the sequence **PLYKKIKKLL**ES or **KKIKKLL**ES.

iv. 25 9. The composition of claim 1 wherein the reagent further comprises a polyvalent linking moiety covalently linked to a multiplicity of the polybasic compounds and also covalently linked to a multiplicity of the technetium-99m binding moieties to comprise a multimeric polyvalent scintigraphic imaging agent, wherein the molecular weight of the multimeric polyvalent scintigraphic imaging agent is less than about 20,000 daltons.

v. 10. The composition according to claim 9 comprising a
multimeric polyvalent scintigraphic imaging agent wherein
35 the polyvalent linking moiety is bis-succinimidylmethyl-
ether, 4-(2,2-dimethylacetyl)benzoic acid, N-[2-(N',N'-
bis(2-succinimido-ethyl)aminoethyl)]-N⁶-N⁹-bis(2-methyl-
2-mercaptopropyl)-6,9-diazanonanamide, tris(succinimidyl-
ethyl)amine, bis-succinimidohexane, 4-(O-CH₂CO-Gly-
H: 40 Gly-Cys.amide)acetophenone or a derivative thereof.

11. An article of manufacture comprising a kit for preparing a radiopharmaceutical preparation, said kit comprising a first sealed vial containing a predetermined quantity of an unlabeled reagent comprising the composition according to claim 1 and a sufficient amount of reducing agent to label the reagent with technetium-99m.

12. The article of manufacture of claim 11, wherein the reducing agent in the first sealed vial is selected from the group of a dithionite ion, a stannous ion, or a ferrous ion.

50 13. The article of manufacture of claim 11 comprising a
second sealed vial containing a predetermined quantity of
the polysulfated glycan, wherein the composition of claim 1
is made by labeling the quantity in the first vial with
technetium-99m and then mixing the contents of the first
55 vial with the contents of the second vial.

14. The article of manufacture of claim 13, wherein the unlabeled reagent and the polysulfated glycan are contained in a single vial.

15. A process of preparing the reagent comprising the
60 composition of claim 1 wherein the reagent is chemically
synthesized in vitro.

16. The process of preparing the reagent according to claim 15 wherein the polybasic compound is a peptide and the peptide is synthesized by solid phase peptide synthesis.

17. The composition of claim 2 wherein the radiolabel binding moiety is covalently linked to the peptide during *in vitro* chemical synthesis.

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18. The composition of claim 17 wherein the radiolabel binding moiety is covalently linked to the peptide during solid phase peptide synthesis.

19. A composition of matter having the formula:

acetyl-KC_{Acm}GC_{Acm}QAPLYKKIHKLLS
 acetyl-KKC_{Acm}GC_{Acm}QAPLYKKIHKLLS
 acetyl-KKKC_{Acm}GC_{Acm}QAPLYKKIHKLLS
 acetyl-KKKKC_{Acm}GC_{Acm}QAPLYKKIHKLLS
 acetyl-KKKKKC_{Acm}GC_{Acm}QAPLYKKIHKLLS
 acetyl-KC_{Acm}GC_{Acm}GGPLYKKIHKLLS
 acetyl-KKC_{Acm}GC_{Acm}GGPLYKKIHKLLS
 acetyl-KKKC_{Acm}GC_{Acm}GGPLYKKIHKLLS

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-continued

acetyl-KKKKC_{Acm}GC_{Acm}GGPLYKKIHKLLS
 acetyl-KKKKKC_{Acm}GC_{Acm}GGPLYKKIHKLLS.

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20. The composition of matter of claim 19 that is labeled with technetium-99m.

21. A composition comprising the composition of matter of claim 19 and a polysulfated glycan.

10

22. The composition of claim 21 that is labeled with technetium-99m.

* * * * *